

INDONESIA





THIS CERTIFICATE IS AWARDED TO

Dr. Paulus Wisnu Anggoro, S.T., M.T.

for presenting paper

Semi Reverse Innovative Design of Insole Shoes Orthotic for Patient with Club Foot

International Biomedical Instrumentation and Technology Conference 2019

Held on October 23^e – 24^e, 2019 ROYAL AMBARRUKMO HOTEL Yogyakarta, Indonesia







The **Empowerment of** Industry 4.0 for **Healthcare and** Welfare Improvement

ISBN: 978-1-7281-3339-3

Royal Ambarrukmo Hotel Yogyakarta, Indonesia | 23 – 24 October 2019





Co-organized with







Kumamoto University

COPYRIGHTS

2019 The 1st International Biomedical Instrumentation and Technology Conference (IBITeC)

Copyright ©2019 by Institute of Electrical and Electronics Engineers, Inc. All rights reserved.

Copyright and Reprint Permission:

Copyright and Reprint Permission: Abstracting is permitted with credit to the source. Libraries are permitted to photocopy beyond the limit of U.S. copyright law for private use of patrons those articles in this volume that carry a code at the bottom of the first page, provided the percopy fee indicated in the code is paid through Copyright Clearance Center, 222 Rosewood Drive, Danvers, MA 01923. For reprint or republication permission, email to IEEE Copyrights Manager at pubs-permissions@ieee.org. All rights reserved. Copyright ©2019 by IEEE.

IEEE Catalog Number : CFP19TEG-ART ISBN : 978-1-7281-3339-3

Link : <u>https://ieeexplore.ieee.org/xpl/conhome/9090219/proceeding</u>

INSTITU	UTIONAL S	UBSCRIBERS: Are you having difficulty accessing IEEE Xplore when working remotely?	Try Theon Time
Eff.org 1997 April	- ere s	A EEE Spectrum More Silve Gart	Create Account Personal Sign In
IEEE Xplore	Browse	❤ My Setings ❤ Help ❤ Institutional Sign In	♦IEEE
	_		
		Barro write McKaller ADNANCED SCARCH	
and the second se			
Biomedical Instrum	entation a	ind Technology Conference (IBITeC), International	- second second
Core Demonst Las		er Tils Litt - 🛱 Versus for Conference Asses	
	1.00		
Proceedings All Proceedings	etings		
2019 International Biom	edical Instru	mentation and Technology Conference (BITeC)	DOI: 10.1100/06/TwC40507.2019
AN ALL NOT AP IN A MARK	Ronso		
Search within results		Per Page: 25 - (E)	port + 1 Email Balacted Results +
Showing 1-25 of 25			
		Select All on Page Sort By: Sequence -	
efine			Nord
uthor	~	A Design of Multipurpose Virtual Reality Game for Children with Autism Spectrum Disorder	Need
		Mila Rahmadiva ; Achmad Arfin ; Muhammad Himon Fatori ; Siti Halmoh Baki ; Takashi	Full-Text
millation	¥	Watanabe Publication Year: 2019. Papelsi: 1 - 6	access to IEEE Xplore
onfarance Location) Abstract html 🖷 (2004 Ka) 💿	for your organization?
		Understremente Sumbaria from Plan Shall Union Understrement Mathed / A Souther	CONTACT IEEE TO SUBSCRIBE
	_	Deni Fajar Fittiyana ; Rifky Ismail ; Yanuar Iman Santosa ; Sri Nugroho ; Ahmad	N AN
UICK LINKS		Jazilussurur Hakim ; Mohammad Syahreza Al Muloj Brativnika Vour 2010, Brancez 7, 11	
earch for Upcoming		Abstract () htmli ()	
CINNEIDIO			IEEED ataPort
EE Publication		 SMILE (Self-Monitoring Interactive Learning Evaluation) for Indonesian University Students 	Manage and store your research
		Wahyul Amion Syafei ; Anastasia Ediati ; D. V. S. Kalooti ; Jati Ariati ; Agung Budi	data with IEEE DataPort
EE Author Center		Prasego; T. E. Windarto; M.A. Vitzawan Publication Year: 2019, Page(s): 12 - 16	Make your datasets easily accessible
		Abstract () html) 🔁 (1201 Ka) C	Link datasets to your
2004 993 997 91	_	Surface Electromycotraphic Signals of Special Needs Children during Fine Motor	IEEE Xplore* paper
roceedings		Task	Increase your citations
he proceedings of this	in for	Publication Year: 2019, Page(s): 17 - 20	
urchase through Curran	e lui	 Abstract () html) (655 Kb) 	Up to 218 data storage
ssociales.		Elavible Windows EPC Circuit Subdivision Tablecista A	Supports open data initiatives
Biomedical Instrumentation		N.S. Sahar; N.A. Abdul-Kadir; F.K. Che Harus	
BITeC), 2019 Internation	nal	Publication Year: 2019, Page(s): 21 - 25	
int on Damand Burnham	-	Andram humil Siloo vei	Participant and

Performance Comparison of Linear and Non Linear Interference Cancellation 0 Techniques for 3.466 Gbps WLAN Wahyut Amien Syatel ; Fathia laralestina ; Catur Edi Widodo Publication Year: 2019, Page(s): 26 - 30 IEEE Abstract () hami () (2) (579 Kb) 0 Optimization of Mechanical Parameters on Outsole Shoes Orthotic Comfort Using 8 Finite Element Analysis Yohanes Eka Anggraita Putra ; Paukai Wianu Anggoro ; Tonny Yuriarto ; A.P. Bayuseno ; Jamari Jamari ; Baju Bawono Publication Year: 2019, Page(s): 31 - 35 Abstract (Listed)
 (1748 Rb) 0 Performance Test of Fingers on 3D Printed Myoelectric Prosthetic Hand 8 Khariuma Agung Pambudi ; Rifky Ismail ; Mochammad Ariyanio ; Joga Dharma Setuavan ; Gilar Pandu Annanto Publication Year: 2019, Page(s): 37 - 40 Abstract 0.mmll (TB/0 Kb) 0 The Effect of Hydroxyapatite-Gelatin Composite with Alendronate as Injectable 8 Bone Substitute on Various Hydroxyapatite-Based Substrate Alfan Pramudita Putra ; Ililyin Faradisa ; Dyah Hikmawati ; Siswanto Publication Year: 2019, Page(s): 41 - 45 Abstract (I New I) 🐑 (925 Kis) 6 Application of CAD / CAM Technology on Facial, Oral and Cranial Region: A Review 8 Rangga Perwiratama ; Margaretha Sulistyoningsih Publication Year: 2019, Page(s): 46 - 51 Abstract (Ment) (575 Kt) 0 Position Control and Trajectory Planning of 3-DOF Arm Manipulator for Test Tube A Handling Hadha Afrisal ; Alfin Lugmanul Hakim ; Muhammad Ja'far Shiddig ; Iwan Setiawan Publication Year; 2019, Page(s); 52 - 57 Abstract (Intml) (601 Kb) C Feature Extraction and Feature Selection Methods in Classification of Brain MRI 8 Images: A Review Aqidatul Izza Poemama ; Indah Soesanti ; Oyas Wahyunggoro Publication Year: 2019, Page(s): 58 - 63) Abstract ((html) 🗐 (71386) 🔘 Evaluation of Kinesthetic/Visual Motor Imagery of Dorsiflexion of the Right Ankle Joint via Event-Related Desynchronization/Synchronization Tomohiko Igasaki ; Arata Shibuta ; Katsuya Sakamoto Publication Year: 2019, Page(s); 64 - 68) Abstract ((html) 🗐 (959 85) 🔘 Performance Evaluation of Ensembles Algorithms in Prediction of Breast Cancer â Gilbert Gutabaga Hungilo ; Gahizi Emmanuel ; Andi W.R. Emanuel Publication Year: 2019, Page(s): 74 - 79 Abstract (I html) (718 Kb) (C) Chitosan-Coated PLLA-Collagen Hollow Fiber for Vascular Graft Engineering Ô Dita Ayu Mayasari ; Prihartini Widiyanti ; Djonny Izak Rudyardjo Publication Year: 2019, Page(s): 80 - 83 Abstract (Mmil) (639 Kb) C 3D Image Reconstruction with Single-Slice CT using Improved Marching Cube â Algorithm Ignatius Luddy Indra Pumama ; Alva Edy Tontowi ; Herianto Herianto Publication Year: 2019, Page(s): 84 - 87 Abstract (I mmil) (771 Kb) (C)



CHANGE USERNAME PASSWORD

PAYMENT OPTIONS

NEW PURCHASED DOCUMENTS

Profile Information

COMMUNICATIONS PREFERENCES PROFESSION AND EDUCATION TECHNICAL INTERESTS

Need Help?

US & CANADA +1 800 678 4330

WORLSWIDE: +1 732 961 0063

CONTACT & SUPPORT

in V

Link : <u>https://ieeexplore.ieee.org/document/9091719/keywords#keywords</u>

Optimization of Using Finite Ele	Mechanical Parameters on Ou ment Analysis	utsole Shoes Orthotic Comfort	Need Full-Text
Publisher: IEEE	Cite This PDF		access to IEEE Xplore for your organization?
6 Author(s) Yohanes E	ka Anggraita Putra ; Paulus Wanu Anggoro ; Tonny Yun	tarto ; A.P. Bayoseno ; Jameri ; Bayu B . All Authors .	REQUEST A FREE TRIAL
			More Like This
Abstract	Abstract: The shoes selection as the right footwear is very	related to the feet comfort, especially in the selection of	Determination of true stress by mage processing based tensile testing machine using Round Continues Arrive bills Neuroscient
Document Sections	shoe materials. The shoe consists of three parts material will affact the contint of feet during activ	Insole; outsole, and upper shoe. The right outsole vity. This paper demonstrates a mechanical testing method.	3017 56th Annual Conference of the Society of Instrument and Control Engineers of Jacen (SICE
i introduction	on optimization of outsole material based on con	nputer aided engineering (CAE). The autoole design on	Puttaned 2017
 Material and methodology 	types of mechanical testing on Abaquis software	2016: bending, torsion, and plantar plessure used in this	New loss for Hydraulic Testing Machine with Stress and Strain Rates Controlled and to
II. Result and discussion	paper to determine the optimal outsole material a that the material EVA rubber type declared with a	2010 Wendonal Conference on Intelligent Concutation Technology and Automation	
W. Conclusion	MPa, maximum principal stress 0.0036 MPa and served as a basic reference for the process of m	I features shock absorption of 5 01562 mJ. This data can unufacturing the outsole of shoe on CNC machines.	Pustaned 2010
Authors			Show Ma
Figures	Published in: 2019 International Biomedical Inc	pumer/ation and technology Conference (IBITeC)	Tour Occupitations with Patents on
Deferences	Date of Conference: 23-24 Oct. 2019	DOI: 10.1109/BITeC46597.2019.9091719	Technologies Mentioned in This Article
References.	Date Added to IEEE Xplone: 14 May 2020	Publisher: IEEE	010446247004+
Keywords	ISBN Information:	Conference Location: Special Region of Yogyakarta, Indonesia, Indonesia	Indunation s
	L Introduction		ORGANIZATION 2
	Footwaar has an important role to protect the t	feet, especially on bottom part, so that they	HIRGANIZATION >
	are not injured when facing do a supporting appearance to a commission of the chroning factors	ntrue Roading	٥
			WORKING FROM
	Autors		HOME?
	Figures	X	
	References	~	
	Keywords	0	Real Provide R
	IEEE Keywords		
	Fortunar Fort Techny Furne Strees Three	dimensional displays. Strain	

Optimization of Mechanical Parameters on Outsole Shoes Orthotic Comfort Using Finite Element Analysis

Yohanes Eka Anggraita Putra Siti Badriyah UNDIP Group Research for Prosthetic and Orthotic, Diponegoro University Semarang, Indonesia Industrial Engineering dept. Atma Jaya Yogyakarta University Yogyakarta, Indonesia anggaeka11@gmail.com

A.P. Bayuseno Siti Badriyah UNDIP Group Research for Prosthetic and Orthotic, Diponegoro University Semarang, Indonesia Mechanical Engineering dept. Diponegoro University Semarang, Indonesia apbayuseno@gmail.com Paulus Wisnu Anggoro Siti Badriyah UNDIP Group Research for Prosthetic and Orthotic, Diponegoro University Semarang, Indonesia Industrial Engineering dept. Atma Jaya Yogyakarta University Yogyakarta, Indonesia pauluswisnuanggoro@ymail.com

Jamari Siti Badriyah UNDIP Group Research for Prosthetic and Orthotic, Diponegoro University Semarang, Indonesia Mechanical Engineering dept. Diponegoro University Semarang, Indonesia jjamari@gmail.com

Abstract—The shoes selection as the right footwear is very related to the feet comfort, especially in the selection of shoe materials. The shoe consists of three parts: insole, outsole, and upper shoe. The right outsole material will affect the comfort of feet during activity. This paper demonstrates a mechanical testing method on optimization of outsole material based on computer aided engineering (CAE). The outsole design on milutes diabetic patients in previous studies used as the basic design for mechanical testing at CAE. Three types of mechanical testing on Abaqus software 2016: bending, torsion, and plantar plessure used in this paper to determine the optimal outsole material as outsole material shoe orthotik. The test results showed that the material EVA rubber type declared with optimum characteristics of the von mises stress 0.0013 MPa, maximum principal stress 0.0036 MPa and features shock absorption of 5.01562 mJ. This data can served as a basic reference for the process of manufacturing the outsole of shoe on CNC machines.

Keywords—comfort, outsole shoe, CAE, FEA, Abaqus 2016

I. INTRODUCTION

Footwear has an important role to protect the feet, especially on bottom part, so that they are not injured when facing diverse environmental conditions. Footwear also functions as a supporting appearance to enhance the performance. The main factors that need to be considered in choosing footwear are comfort, where these factor are a combination of physical processes, physiological and psychological aspects [1-4].

Wrong choice of footwear is bad for our health, especially foot health. When someone uses wrong and not needed footwear (according to foot geometry and material), it can increases the risk of injury. In addition, it can also cause various kinds of diseases such as inflammation of the tissues in the lower legs, hardening of the skin, and even pain in the lower back. Therefore, it is highly recommended to choose footwear that suits the needs and shape of the user's feet. Tonny Yuniarto Siti Badriyah UNDIP Group Research for Prosthetic and Orthotic, Diponegoro University Semarang, Indonesia Industrial Engineering dept. Atma Jaya Yogyakarta University Yogyakarta, Indonesia tonnyyuniarto@gmail.com

Baju Bawono Siti Badriyah UNDIP Group Research for Prosthetic and Orthotic, Diponegoro University Semarang, Indonesia Industrial Engineering dept. Atma Jaya Yogyakarta University Yogyakarta, Indonesia bajubawono@gmail.com

Shoes and sandals have been made in several variants based on aspects of the needs and shape of human feet. Shoes consist of three parts, namely upper, insole and outsole [5, 6]. These parts have their respective function. The upper is a foot cover that protects it from outside danger. Insole has a function to maintain balance in body posture. While the outsole functions to grip the surface of the ground and prevent damage to the midsole as reported [7, 8]. Outsole or known as shoe sole, is the bottom of the shoe that is directly in contact with the ground. In order to function properly when used, outsole as explained [7, 8] is generally made of rubber material. This material type, generally has ability to grip properly, but has different characteristics. Polyurethane has better machineability but harder so the assembly process with upper will take longer [9, 10]. EVA rubber type also can be used as an outsole with softer characteristics which has an impact on the machineability is not good, but it easier to sew with the upper so it can be processed faster [6, 8].

The use of these two material types as an outsole in the orthotic shoe manufacturing process has been done by several researchers, but most only discussed is about materials manufacturing aspects in CNC machines and rarely discuss about aspects of outsole designs optimization in both materials [8, 9, 10]. In fact, according to previous research, the type of material and footwear's geometry is very influential on the characteristics of footwear deformation despite only discussing on the standard outsole form [11]. This means that these two factors are significant in choosing comfortable footwear.

Finite element analysis (FEA) is one of the numerical methods that often used by Computer Aided Engineering (CAE) engineers for multi-dimensional and asymmetric problem solving to estimate an optimal solution before the manufacturing process on CNC or 3D printing machines [9, 12, 13]. FEA tool also can be used to determine design optimization of a product or component at design or development stage of innovative designs, especially based on reverse innovative design (RID) such as developed [14, 15].

The definition of comfort is clearly stated [1-3, 16] as "lack of pain" and "a happy feeling of health and well-being" needed by patient and this is situationally (against reactions made by patients) which consists of physiological, psychological and physical aspects. The skeleton parts of the foot defined in a simple form built from other softer tissues. Feet are parts of the human body that located at the far end and significantly accept all loads. Overloading on feet can be a cause of discomfort, pain and actual injury to human's body part. Interaction or direct mechanical contact between feet and soil can occur directly or use footwear consisting of one or more parts of footwear. Here, the bottom of the foot will receive a full or significant load through contact mechanics on the plantar side of the foot with the soil.

The definition of mechanical comfort [1, 17-19] can be divided into two, namely plantar and dorsal mechanical comfort. Plantar mechanics of standing and gait are very important for the rough mechanics of the body and are discussed in several works.

In detail of previous research [2, 19, 20], has already stated that the most important problem in the plantar mechanics is the ground reaction force to the action of the weight as shown in Fig. 1. On this picture, it looks that normal vector (the influence of force that occurs against the surface of the foot plantar) of this force is greater than the vector of transverse and lengthwise.



Fig. 1. Force during gait (IC = Initial Contact, OT = Opposite Toe Off, HR = Heel Rise, OI = Opposite Initial Contact, TO = Toe off, FA = Feet Adjacent, TV = Tibia vertical) [1]

The use of FEA modeling and extensive to do the actual measurement, calculation or estimation of normal plantar force has also been done by some researchers [1, 9, 12, 21, 22, 24]. The effects of normal plantar force happen at the level of discomfort, pain and injury are significant when sliding force vector quantity resulting from mechanical contact is limited. Even though in the end this will cause to happen tissue damage in the feet.

This paper discusses the application of FEA to evaluate performance in terms of comfort outsole mechanics based on simulation testing of bending, torsion, and plantar pressure (contact mechanics between the legs with the outsole). The simulation stage is based on FEA with the help of CAE software from the shoe structure which is treated according to their performance restrictions and combined with a simpler human foot detail Biomodel.

II. MATERIAL AND METHODOLOGY

One DM patient is defined in this paper for the manufacture process of insole and outsole using the RID method [8]. 3D outsole design obtained from the insole of high risk scale diabetic patient foot on Fig. 2 [10], actually still needs to be simplified on the rocker arm [24, 25]. This simplification is being done by researchers according to needs and without compromising the essence of design [12]. The simplification results can be presented in Fig. 3.



Fig. 2. The 3D (a) left insole, (b) left outsole, (c) right insole, (d) right outsole [8]



Fig. 3. Revised 3D outsole shoes orthotic for diabetic patients: (a) right foot; (b) left foot; (c) isometric view [27]

FEA process with the CAE software (Abaqus 2016) in this paper is done with three types of testing (bending, torsion, and plantar pressure) based on six types of material data (PU, EVA A, EVA D, EVA E, ABS, and PVC). Outsole material data that will be performed contact mechanics can be presented in Table I. Based on previous research [1, 11], testing can take one of the right or left leg samples as it is essentially for material analysis to require only basic shapes. The stage of contact mechanics testing with Abaqus 2016 is based on the order of modules in the software and presented in Fig. 4. The parameters of the three types of tests are set to resemble previous research [1] But some adjustments were made to face the new test conditions.

Bending testing on this research using 2 boundary conditions, there are the front bottom of 3D outsole is set as fixed area along 26% of the total length of the outsole, then the back is bent upward until it makes a maximum angle of 55° . As for the torsion testing, the heel area of the 3D outsole is twisted by 15° and fixed the same area on the bending test. Furthermore, the testing of plantar pressure, all over the bottom surface of the 3D outsole is used as a fix area by providing a load 340 kN with 3D model foot form. The size of 3D outsole mesh in this study is 7 which more thorough than the previous research is 10, while the 3D mesh size of the foot model is 2. Because of the difference in the mesh size, when the assembly process uses the dependent instance type.

The results of three tests from this research in the form of fringe diagrams presented in Fig. 5 - Fig. 7. The data from the chart included in Table II - Table IV for easy benchmarking of material characteristics. In addition, testing bending and

torsion also produces stress-strain curve, whereas the testing of plantar pressure generating reaction force - displacement, reaction force - pressure stress, and strain energy pertime period curves.

TABLE I. MATERIAL DATA FOR TEST

Material	Young's Modulus (GPa)	Poisson's Ratio	Mass Density (kg/m3)	Description
EVA A	0.0094	0.49	80.8310	
EVA D	0.01464	0.49	138.3024	
EVA E	0.01035859	0.49	181.9600	
PU	2.07	0.3	1240	
ABS	2.9	0.40	1015	
PVC	4.14	0.42	1400	
Foot	937	0	1.15	Indenter
Stainless Steel	200	0.27	7800	Indenter



Fig. 4. Contact Mechanics Testing Using Abaqus 2016



Fig. 5. Fringe diagrams of von mises stress for: (a) PU, (b) ABS, (c) PVC, (d) EVA A, (e) EVA D, (f) EVA E on bending test [27]



Fig. 6. Fringe diagrams of von mises stress for: (a) PU, (b) ABS, (c) PVC, (d) EVA A, (e) EVA D, (f) EVA E on torsion test [27]



Fig. 7. Distribution of plantar contact pressure for: (a) PU, (b) ABS, (c) PVC, (d) EVA A, (e) EVA D, (f) EVA E [27]



Fig. 8. Stress-Strain Curve from Bending and Torsion Test, Material : PU, ABS, and PVC; Type A, D, and E, EVA rubber [27]

	s	Stress	Logarithmic Strain
Material	Von Mises (MPa)	Max. Prin. Abs. (MPa)	Max. Prin. Abs.
PU	1.24552	1.13783	0.455304
EVA A	0.00751238	0.0120893	0.426745
EVA D	0.0117001	0.0188285	0.426745
EVA E	0.00827848	0.0133222	0.426745
ABS	1.74625	1.84954	0.442026
PVC	2.53001	2.80579	0.442145

TABLE III. STRAIN-STRESS FROM TORSION TEST

Material	S	itress	Logarithmic Strain
	Von Mises (MPa)	Max. Prin. Abs. (MPa)	Max. Prin. Abs.
PU	0.322894	0.355109	0.202296
EVA A	0.00133259	0.00366398	0.164172
EVA D	0.00207545	0.00570646	0.164172
EVA E	0.00146849	0.00403763	0.164172
ABS	0.433237	0.711036	0.196587
PVC	0.611856	1.06547	0.193729

 TABLE IV.
 Plantar Contact Pressure, Reaction Force, and Strain Energy from Plantar Pressure Test

Material	Plantar Contact Pressure (MPa)	Reaction Force (x10 ⁻⁸ kN)	Strain Energy
PU	4503.39	1.2489	45.7867
EVA A	906.725	0.995418	5.01562
EVA D	1144.48	1.11817	8.76533
EVA E	1188.1	0.602554	10.4532
ABS	3509.23	4.94235	47.3498
PVC	5058.73	5.85597	54.0731



IBITeC 2019 - Page 34 of 135 Authorized licensed use limited to: Univ of Calif Santa Barbara. Downloaded on May 16,2020 at 02:29:08 UTC from IEEE Xplore. Restrictions apply.



Fig. 9. Reaction Force - Displacement curve from plantar pressure test [27]



Fig. 10. Reaction Force – Pressure Stress curve from plantar pressure test [27]



Fig. 11. Strain Energy pertime periode curve from plantar pressure test [27]

III. RESULT AND DISCUSSION

Simplification and improvements can be made in 3D design (Fig. 2 - Fig. 3) according to the requirement and without compromising its essence [12]. This is done because of the required regularity of mesh in 3D design so that it can be solved by FEA. Mesh size variation that is too large and not neat will affect simulated result data is less valid. It is because the calculation on each mesh is uneven. On the other hand, it will cause the analysis process longer and make excessive burden on the hardware.

As an initial step in testing, 3D outsole design that is fixed exported with STEP (STandard for the Exchange of Product) format and then imported into the Abaqus 2016 through part module. The same thing is done on the 3D model patient foot who already scanned in plantar pressure testing. The STEP format is selected because it is a high-profile replacement for format IGES (Initial Graphics Exchange Specification) that can be imported into all programs CAD, CAM, and CAE globally [26].

Fringe diagram of von mises stress (Fig. 5 - Fig. 6) shows the area of the occurrence of the failure that is marked with the color code. Red color indicates the critical area. According to von mises stress value in Table II and Table III, the failure rate is the largest PVC material with 2.53001 MPa on testing bending and torsion test at 0.611856 MPa. Meanwhile, EVA rubber type A has the smallest value with 0.00751238 MPa on testing bending and torsion test at 0.00133259 MPa. Stress-strain curve in Fig. 8, on all types of materials have a constant ride pattern, which means the bigger the change form the great force of working. From the curve can be seen that the PVC material is stated as the most rigid while the EVA rubber type with the most flexible. Flexibility indicates the ability to follow foot movements during activities.

Interaction in the case of contact mechanics between legs with 3D outsole is displayed in the distribution of plantar contact pressure (Fig. 7) with the red color code indicating the largest pressure area. According to Table IV, it is known that the combination of the foot with PVC material has the highest plantar contact pressure value of 5058.73 MPa or 5.6 times greater than EVA rubber type A material that only 906,725 MPa. Displacement of the legs will cause a reaction force on the outsole depicted in Fig. 9. Then, the reaction force is again causing pressure stress on the legs that are seen in Fig. 10. Outsole with PVC material has the biggest reaction force that is 5.85597x10⁻⁸ kN at displacement foot 0.114947 mm and resulted in a pressure stress of 0.903628 MPa. It can be interpreted that PVC material will be difficult to follow the contour of the foot because it has a strong tendency to return to the initial form when stepped on. In contrast, the EVA rubber type A material is easier to follow the contour of the foot because of its smallest reaction force of 9.95418x10⁻⁹ kN at displacement foot 0.50137 mm and resulted in pressure stress of 0.164489 MPa on the foot.

The curve of strain energy as a parameter to represent the shock absorption that is the ability of the material to absorb energy shock when the standing position [1]. The greater the energy that occurs may imply that worse shock absorption. Based on this research, EVA rubber type is declared to have be the best shock absorption because it has smallest energy strain that is 5.01562 mJ.

IV. CONCLUSION

Based on the analysis results, it is concluded that the comfort of foot mechanics can be reviewed by testing bending, torsion, and plantar pressure on the design of 3D outsole to obtain mechanical characteristics of each material such as stress, strain, and Shock absorption. Material EVA Rubber Type A is expressed as material that has the characteristics of qualified to be expressed optimally in the comfort of mechanical. It is able to follow the movement of the foot when worn and have the best shock absorption.

Factors affecting the mechanical comfort based on Finite Element Analysis (FEA) are stress, strain, and shock absorption. Initial data in the form of the basic properties of the material as the mass density, poisson's ratio, and young's modulus is required to get these factors. The optimal 3D outsole design also affects FEA because of the calculated value of mechanical comfort factor based on the element and the point in the design.

V. ACKNOWLEDMENT

This paper can be solved because it is funded by the Directorate of Research and Community Service, strengthening of the Directorate General of Research and Development, Ministry of Research Technology and Higher Education of the Republic of Indonesia Year 2019 No. 257-93 / UN7 / P4.3 / PP / 2019 and No. 257-73 / UN7 / P4.3 / PP / 2019

REFERENCES

- Papagiannis, Panagiotis, Koutkalaki, Z., Azariadis, P., & Papanikos, P. (2015). Definition and evaluation of plantar mechanical comfort for the support of footwear design. Computer-Aided Design and Applications, 13, 162–172. https://doi.org/10.1080/16864360.2015.1084189
- [2] Au, E., & Goonetilleke, R. (2005). Comfort Characteristics of Ladies' Dress Shoes, Technical Report - Project No: HKUST 6162/02E, Hong Kong.
- [3] Fan, J. (2009). Physiological comfort of fabrics and garments. In Engineering Apparel Fabrics and Garments (pp. 201–250). https://doi.org/10.1533/9781845696443.201
- [4] Vink, P.; Looze, M. P. D.; Kuijt-Evers, L. F. M.: Theory of Comfort, in: Vink P. (ed) Comfort and Design: Principles and Good Practice, CRC Press, Boca Raton, Florida, 2005. http://dx.doi.org/10.1201/9781420038132.ch2
- [5] Promjun, S., & Sahachaisaeree, N. (2012). Factors Determining Athletic Footwear Design: A Case of Product Appearance and Functionality. Procedia - Social and Behavioral Sciences, 36, 520–528. https://doi.org/10.1016/j.sbspro.2012.03.057
- [6] Chapman, J. D., Preece, S., Braunstein, B., Höhne, A., Nester, C. J., Brueggemann, P., & Hutchins, S. (2013). Effect of rocker shoe design features on forefoot plantar pressures in people with and without diabetes. Clinical Biomechanics (Bristol, Avon), 28(6), 679–685. https://doi.org/10.1016/j.clinbiomech.2013.05.005
- [7] Mills, N. J. (2003). Running shoe materials. In Materials in Sports Equipment (pp. 65–99). https://doi.org/10.1533/9781855738546.1.65
- [8] Anggoro, P. W. (2018). Aplikasi Computer Aided Reverse Engineering System (CARESystem) dalam Tahapan Desain dan Manufaktur Sepatu Orthotik (Desertasi). Universitas Diponegoro, Semarang, Jawa Tengah.
- [9] Anggoro, P. W., Saputra, E., Tauviqirrahman, M., Jamari, J., & Bayuseno, A. P. (2017). A 3-dimensional finite element analysis of the insole shoe orthotic for foot deformities. International Journal of Applied Engineering Research, 12(15), 5254–5260.
- [10] Anggoro, P. W., Tauviqirrahman, M., Jamari, J., Bayuseno, A. P., Bawono, B., & Avelina, M. M. (2018). Computer-aided reverse engineering system in the design and production of orthotic insole shoes for patients with diabetes. Cogent Engineering, 5, 1–20. https://doi.org/10.1080/23311916.2018.1470916
- [11] Papagiannis, P, Azariadis, P., & Papanikos, P. (2017). Evaluation and optimization of footwear comfort parameters using finite element analysis and a discrete optimization algorithm. IOP Conference Series: Materials Science and Engineering, 254, 162010. https://doi.org/10.1088/1757-899X/254/16/162010
- [12] Cheung, J. T.-M., & Zhang, M. (2005). A 3-dimensional finite element model of the human foot and ankle for insole design. Archives of Physical Medicine and Rehabilitation, 86(2), 353–358. https://doi.org/10.1016/j.apmr.2004.03.031

- [13] Davia-Aracil, M., Jimeno-Morenilla, A., & Salas, F. (2016). A new methodological approach for shoe sole design and validation. The International Journal of Advanced Manufacturing Technology, 86(9– 12), 3495–3516. https://doi.org/10.1007/s00170-016-8427-5
- [14] Ye, X., Liu, H., Chen, L., Chen, Z., Pan, X., & Zhang, S. (2008). Reverse innovative design — an integrated product design methodology. Computer-Aided Design, 40(7), 812–827. https://doi.org/10.1016/j.cad.2007.07.006
- [15] Anggoro, P. W., Tauviqirrahman, M., Jamari, J., & Bayuseno, A. P. (2019). CNC Milling of EVA FOAM with Varians Hardness for Custom Orthotic Insole Shoes and Process Parameter Optimization. Journal Mechanical Engineering and Sciences.
- [16] Kuijt-Evers, L., de Looze, M., & Vink, P. (2004). Theory of Comfort. In P. Vink (Ed.), Comfort and Design (pp. 13–32). https://doi.org/10.1201/9781420038132.ch2
- [17] Keller, T., Weisberger, A., Ray, J., Hasan, S., Shiavi, R., & Spengler, D. (1996). Relationship between vertical ground reaction force and speed during walking, slow jogging, and running. Clinical Biomechanics, 11(5), 253–259. https://doi.org/10.1016/0268-0033(95)00068-2
- [18] Kirtley, C. (2006). Clinical gait analysis: Theory and practice. Retrieved from http://books.google.com/books?id=sOtqAAAAMAAJ
- [19] Whittle, M. (2007). Gait analysis an introduction. Retrieved from http://www.sciencedirect.com/science/book/9780750688833
- [20] Keijsers, N. (2012). Plantar Pressure Analysis. In R. Goonetilleke, The Science of Footwear (Vol. 20124334, pp. 377–408). https://doi.org/10.1201/b13021-23
- [21] Erdemir, A., Saucerman, J. J., Lemmon, D., Loppnow, B., Turso, B., Ulbrecht, J. S., & Cavanagh, P. R. (2005). Local plantar pressure relief in therapeutic footwear: Design guidelines from finite element models. Journal of Biomechanics, 38(9), 1798–1806. https://doi.org/10.1016/j.jbiomech.2004.09.009
- [22] Goske, S., Erdemir, A., Petre, M., Budhabhatti, S., & Cavanagh, P. R. (2006). Reduction of plantar heel pressures: Insole design using finite element analysis. Journal of Biomechanics, 39(13), 2363–2370. https://doi.org/10.1016/j.jbiomech.2005.08.006
- [23] Shariatmadari, M. R., English, R., & Rothwell, G. (2010). Finite Element Study into the effect of footwear temperature on the Forces transmitted to the foot during quasi- static compression loading. IOP Conference Series: Materials Science and Engineering, 10, 012126. https://doi.org/10.1088/1757-899X/10/1/012126
- [24] Bathe, K.-J. (1996). Finite element procedures. Englewood Cliffs, N.J: Prentice Hall.
- [25] Hughes, T. J. R. (2000). The finite element method: Linear static and dynamic finite element analysis. Mineola, NY: Dover Publications.
- [26] Dassault Systèmes. (2015). Abaqus 2016 Documentation. Retrieved from http://130.149.89.49:2080/v2016/index.html
- [27] Putra, Y. E. A. (2019). Evaluasi Dan Optimalisasi Material Outsole Menggunakan Finite Element Analysis. (Skripsi). Universitas Atma Jaya, Yogyakarta, Indonesia.

IBITeC 2019 - Page 36 of 135